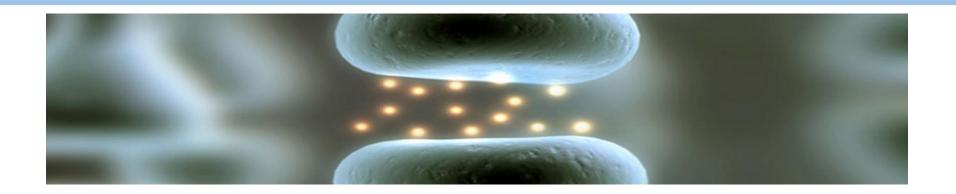




Implants designed to restore sensorimotor functions



Thomas Guiho – October 6th 2023 M2 – Bionic – Part II thomas.guiho@inria.fr – CAMIN team (INRIA)





Implants designed to restore sensorimotor functions





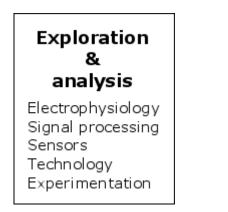
A - CAMIN team ?

INRIA : National Institute for Research in Digital Science and Technlogy

Based in Montpellier and attached to the Sophia Antipolis center

CAMIN : Dedicated to **Neuroprostheses**

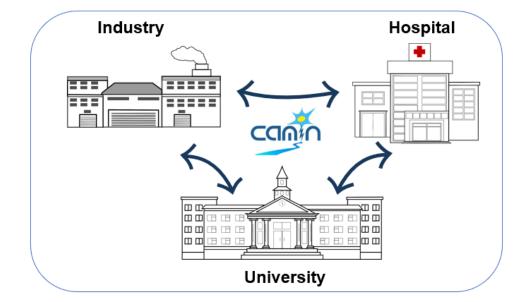
Axes of research :

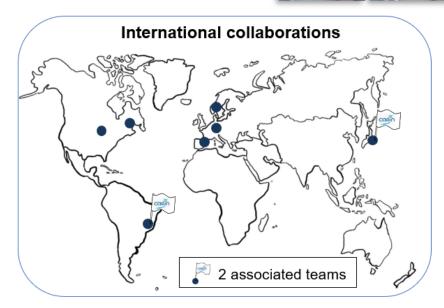




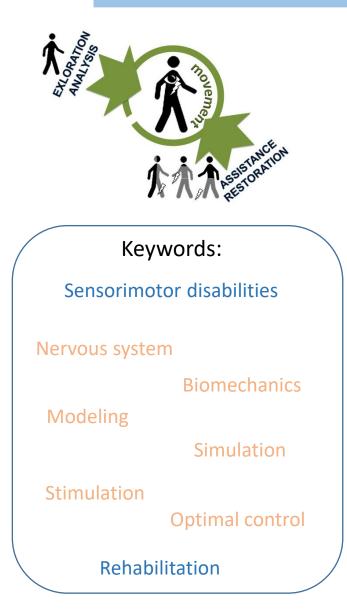


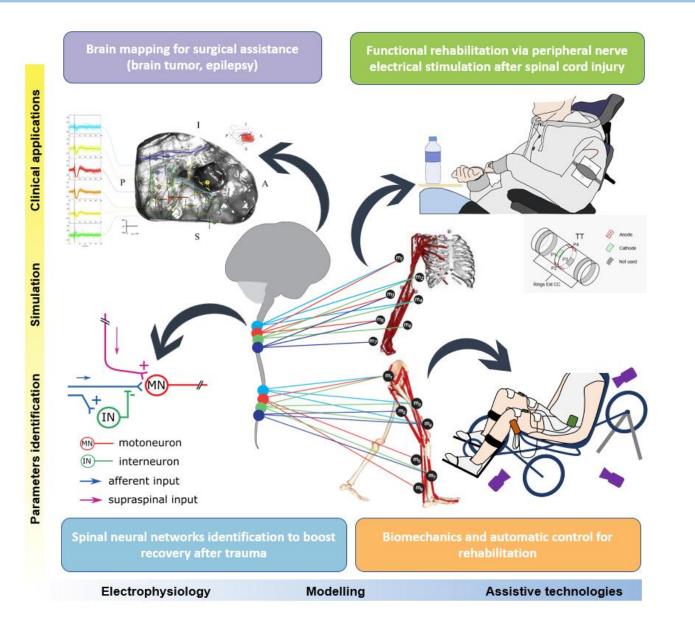


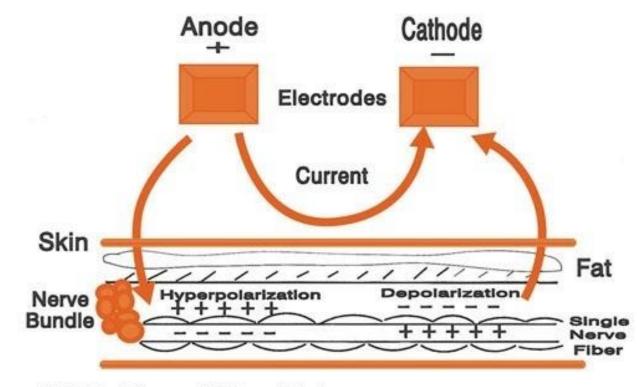




4





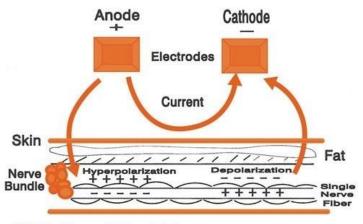


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Direct Current (DC) – Galvanic

Continuous unidirectional flow of charged particles with a duration of at least 1 second.

One electrode is always the anode (+) and one is always the cathode (-) for the entire event.



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There is a build-up of charge since it is moving in one direction causing a strong chemical effect on the tissue under the electrode

"High Volt", "HVGS", "ESTR", and "Iontophoresis" are clinical examples of direct current forms of stimulation

Note : **Monophasic** also refers to direct current, but it is typically pulsed, so the chemical effect is minimal

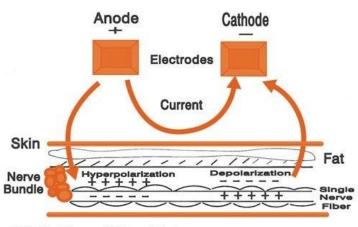
Alternating Current (AC) – Biphasic

Continuous changing voltage level and direction; direction changes at least once per second.

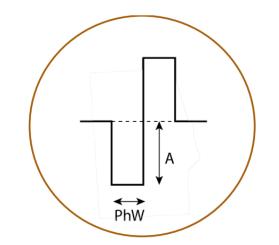
Electrodes continuously alternate their polarity each cycle, therefore no build-up of charge under the electrodes

Alternative current "waves" can be symmetrical or asymmetrical

"Russian", "NMES", "FES", and "TENS" are clinical examples of alternating current forms of stimulation

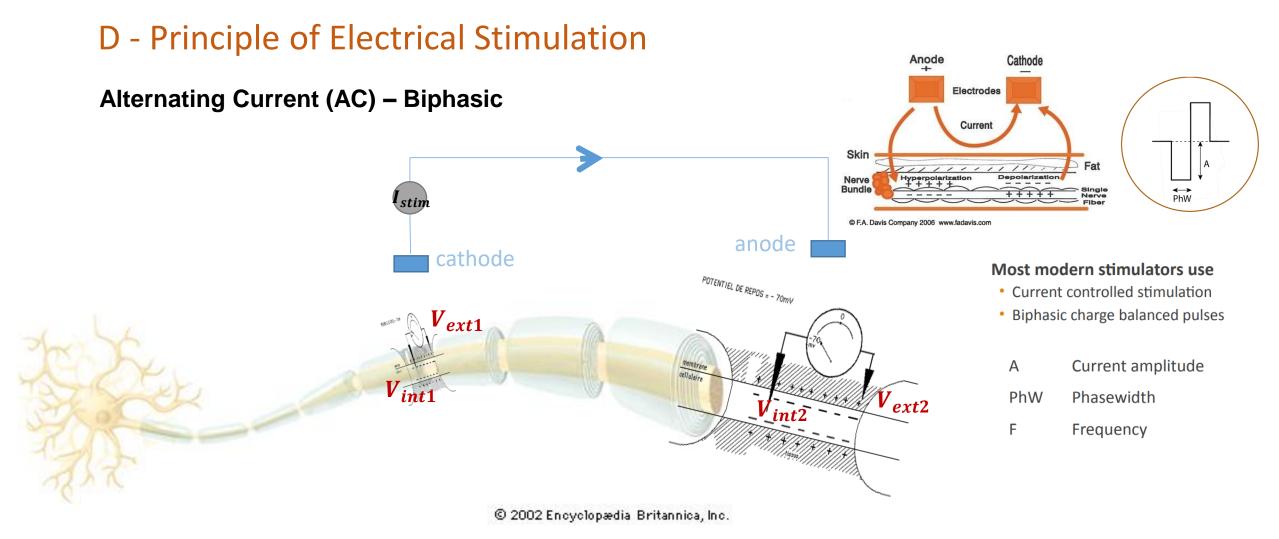


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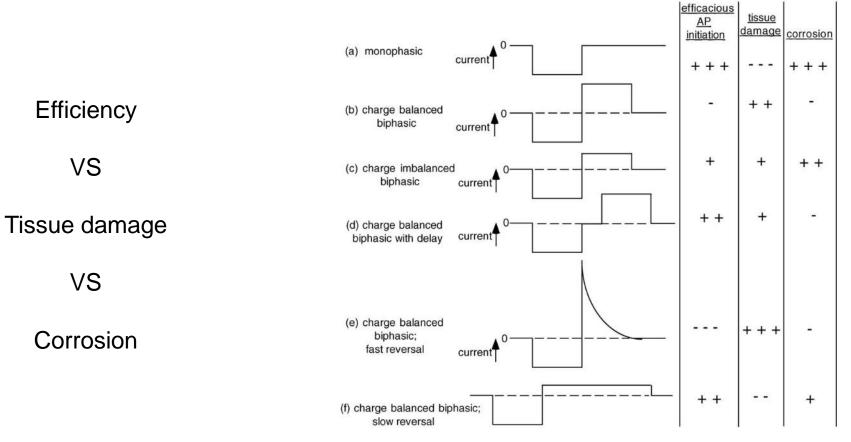


Most modern stimulators use

- Current controlled stimulation
- Biphasic charge balanced pulses
- A Current amplitudePhW PhasewidthF Frequency



Direct Current (DC) VS Alternating Current (AC)



From Merrill et al., Journal of Neuroscience Methods. 2004.





Implants designed to restore sensorimotor functions

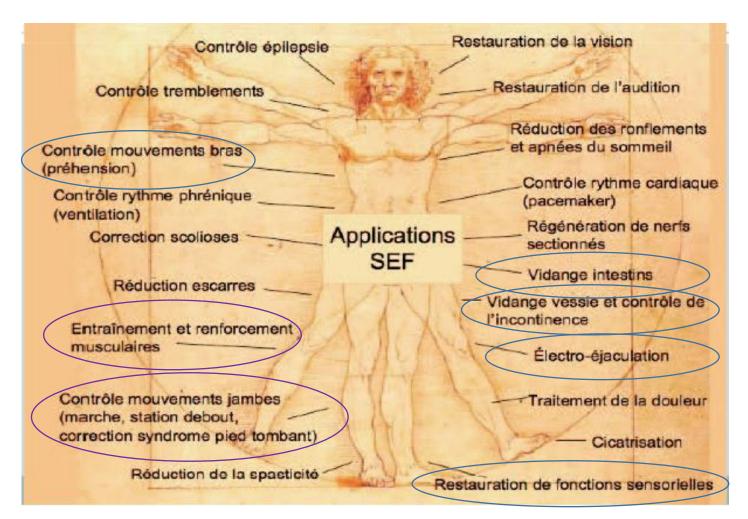


Introduction – Neuroprotheses?

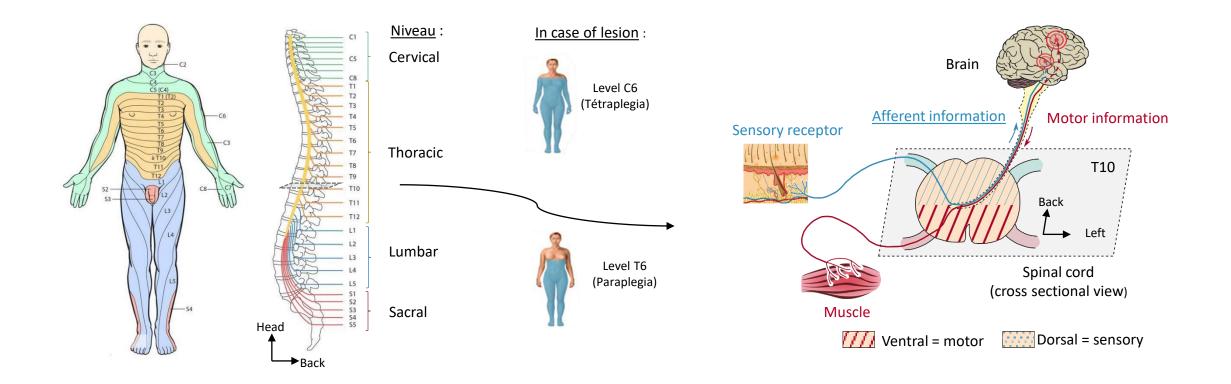
Application domains Marketed technologies Research perspectives

Beyond stimulation...

Areas of application



In a context of spinal cord injuries (SCI)







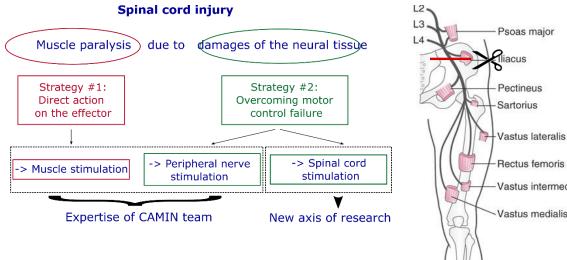
Implants designed to restore sensorimotor functions

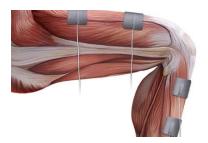


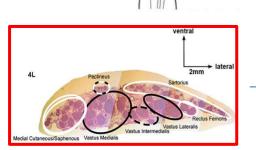
Introduction – Neuroprotheses? Application domains Marketed technologies Research perspectives Beyond stimulation...

Target <-> Selectivity

Periphery:







Psoas major

iacus

Pectineus

Sartorius

-Rectus femoris

Vastus medialis

Vastus intermedius

[1]

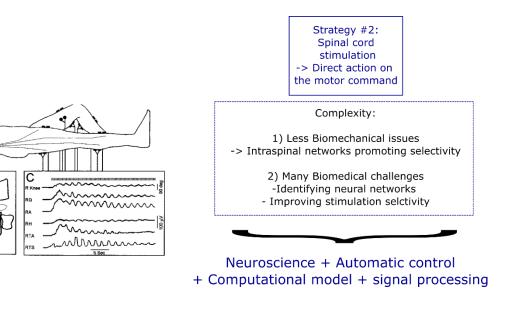
[2]

А

IDEL

LOOD S

Central Nervous System:



PNS - Promising but selectivity issues

Peripheral Nerve Stimulation

Cuff Electrodes in a context of SCI

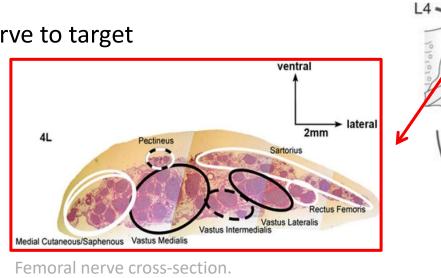
Approach developped in the team – Peripheral Nerve Stimulation

Ability to activate specific fibres within the nerve to target specific functions

Spatial selectivity

Selectivity to direction of propagation

Selectivity to fibre diameter



Gustafson, Kenneth J., et al. "Fascicular anatomy of human femoral nerve: implications for neural prostheses using nerve cuff electrodes." *Journal of rehabilitation research and development* 46.7 (2009): 973.

=> Avoid activating undesirable afferent or efferent functions

Muscular distribution of the femoral nerve Moore& Roy, Rapid Review Gross and Developpement Anatomy © Elsevier 17

Psoas major

Iliacus

- Pectineus

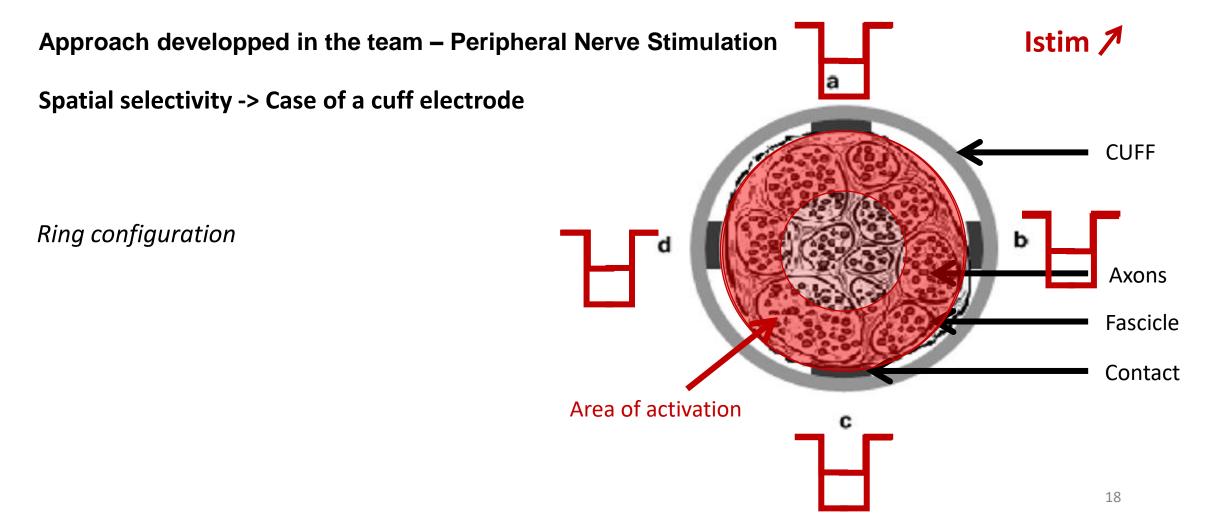
Sartorius

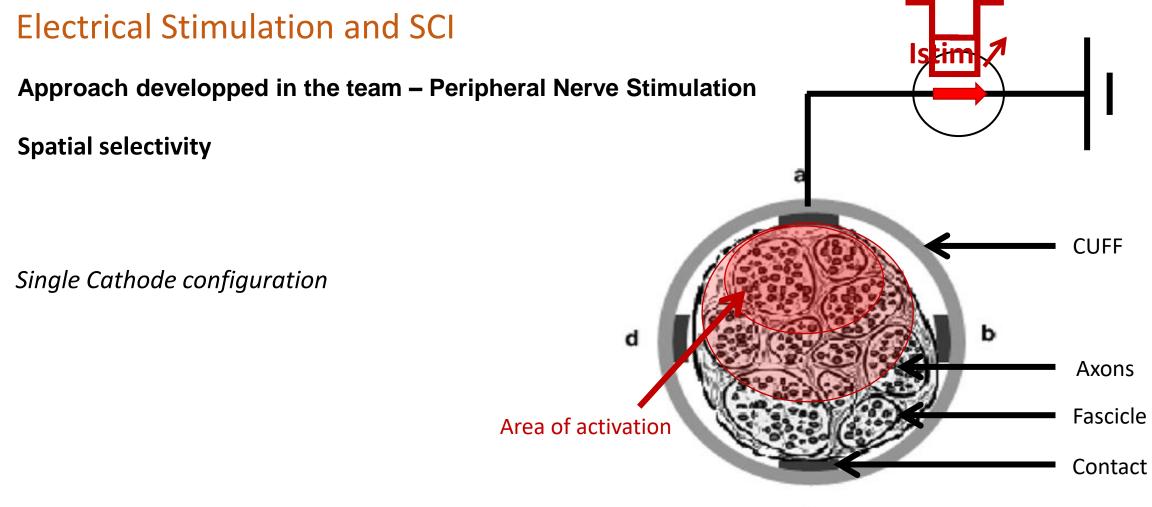
-Vastus lateralis

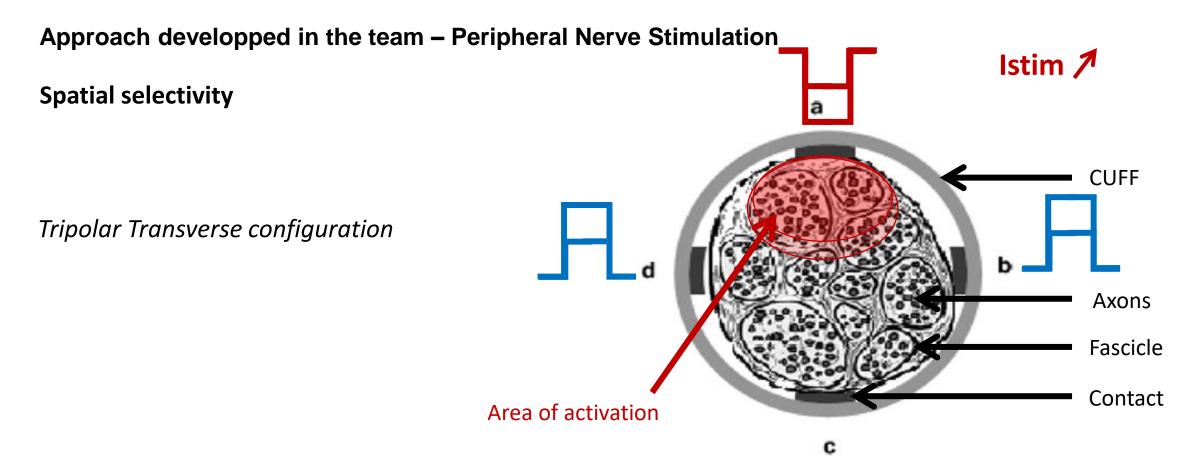
Rectus femoris

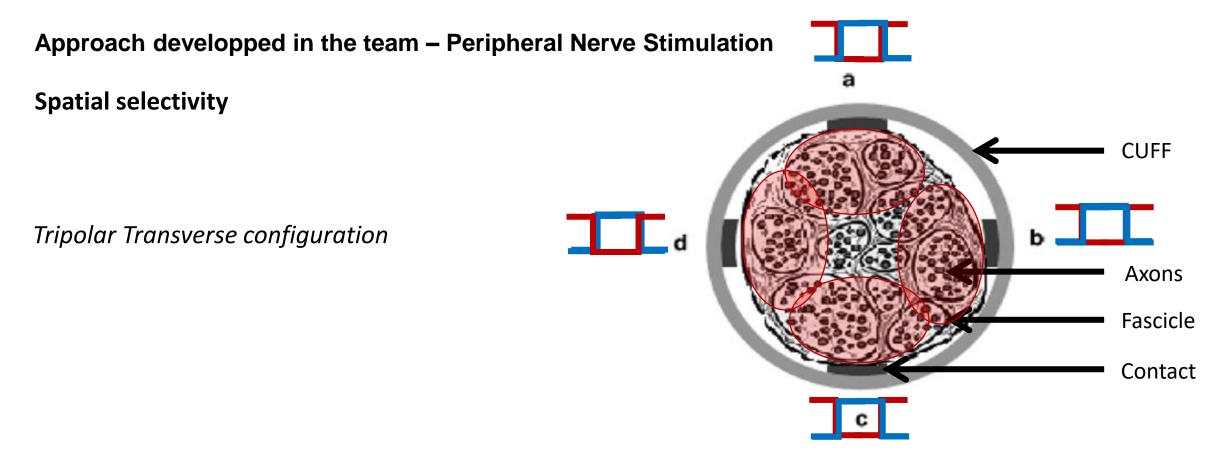
Vastus medialis

Vastus intermedius



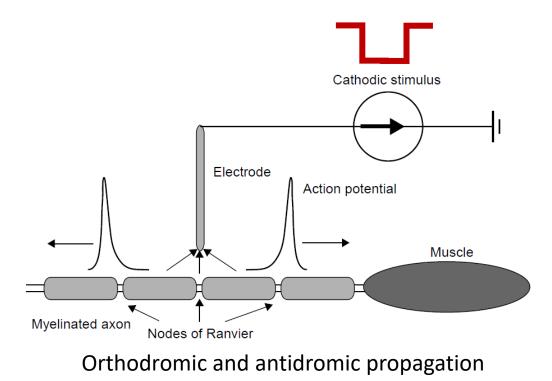


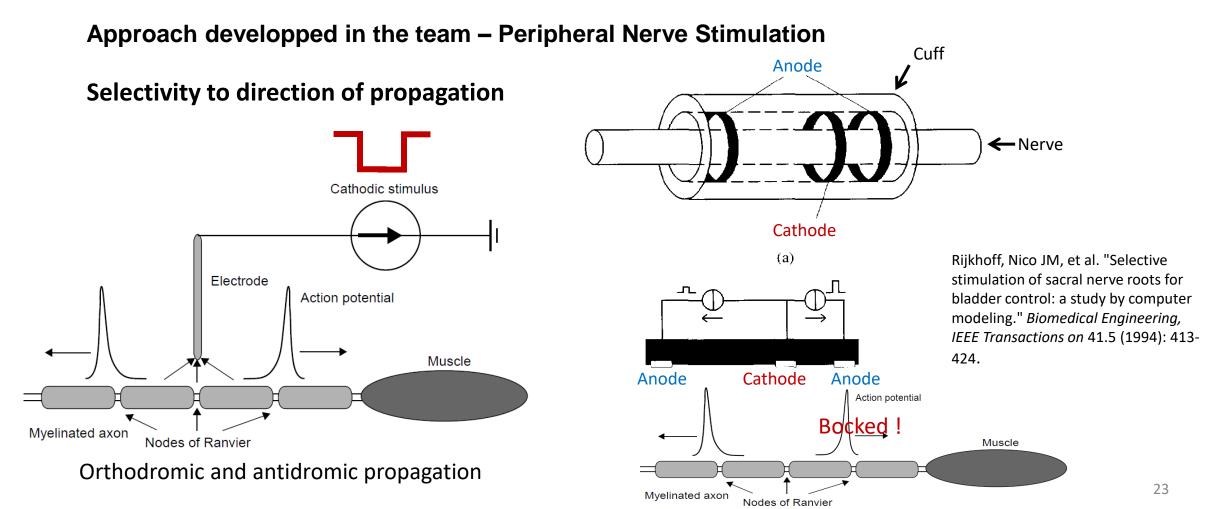




Approach developped in the team – Peripheral Nerve Stimulation

Selectivity to direction of propagation





Approach developped in the team – Peripheral Nerve Stimulation

Selectivity to fibre diameter

Properties of motor units

Muscle Fibers			
Twitch properties	Slow	Fast	
Metabolic properties	Oxidative	Oxidative/ glycolytic	Glycolytic
Name based on twitch and metabolic properties	SO	FOG	FG
Other nomenclature	ST, Type I	FTa, FTA, Type IIA	FTb, FTB, Type IIB
Motor Neurons			
Neuron type	α2	α1	α1
Neuron size	Small	Large	Large
Conduction velocity	Slow	Fast	Fast
Recruitment threshold	Low	High	High

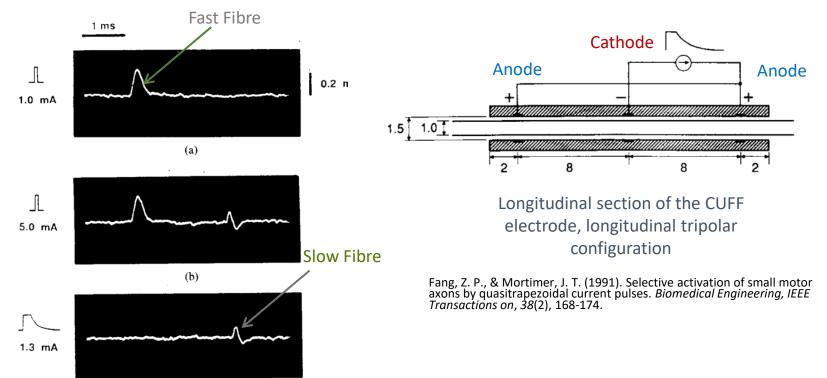
Approach developped in the team – Peripheral Nerve Stimulation

(c)



Action potentials of two fibres: fast (120 m/s) and slow (40 m/s).

1mA rectangular pulse: activation of the fast fibre5mA rectangular pulse: activation of both fibresQuasitrapezoidal pulse: activation of the slow fibre



25

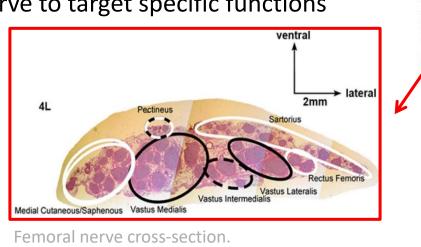
Approach developped in the team – Peripheral Nerve Stimulation

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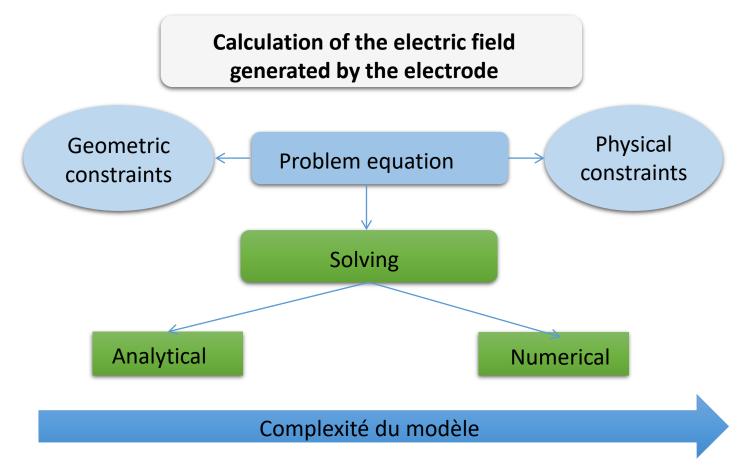
Gustafson, Kenneth J., et al. "Fascicular anatomy of human femoral nerve: implications for neural prostheses using nerve cuff electrodes." *Journal of rehabilitation research and development* 46.7 (2009): 973.

Psoas major Iliacus - Pectineus Sartorius Vastus lateralis Rectus femoris Vastus intermedius Vastus medialis

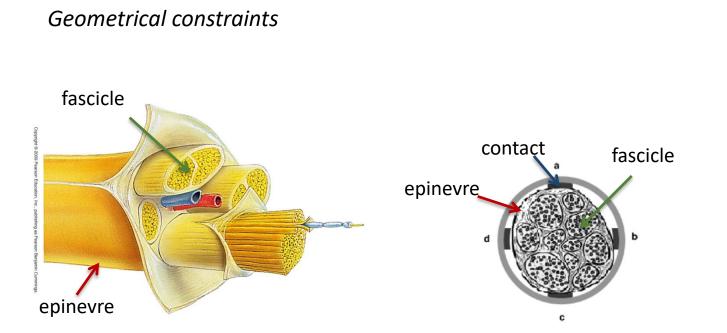
=> How can we improve the selectivity of Peripheral Nerve Stimulation

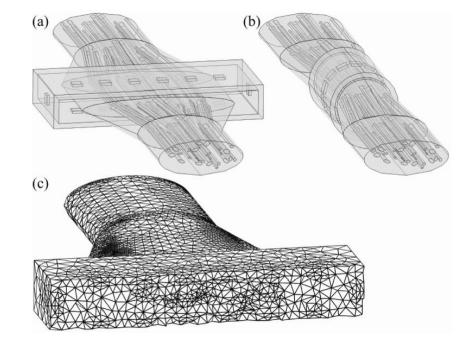
Muscular distribution of the femoral nerve Moore& Roy, Rapid Review Gross and Developpement Anatomy © Elsevier 26

Peripheral Nerve Stimulation and modelling



Peripheral Nerve Stimulation and modelling





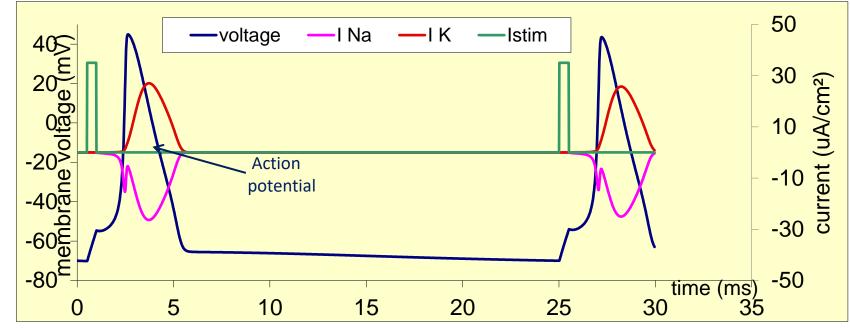
Finite element model of the surrounding tissues

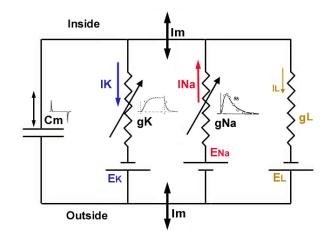
Nerve and electrode to be modelled

Peripheral Nerve Stimulation and modelling

Physical constraints – Example: Hodgkin Huxley

$$\begin{split} C \frac{dv}{dt} &= I - g_{Na} m^3 h(V - V_{Na}) - g_K n^4 (V - V_K) - g_L (V - V_L) \\ \frac{dm}{dt} &= a_m (V)(1 - m) - b_m (V)m \\ \frac{dh}{dt} &= a_h (V)(1 - h) - b_h (V)h \\ \frac{dn}{dt} &= a_n (V)(1 - n) - b_n (V)n \\ a_m (V) &= .1(V + 40)/(1 - \exp(-(V + 40)/10)) \\ b_m (V) &= 4 \exp(-(V + 65)/18) \\ a_h (V) &= .07 \exp(-(V + 65)/20) \\ b_h (V) &= 1/(1 + \exp(-(V + 35)/10)) \\ a_n (V) &= .01(V + 55)/(1 - \exp(-(V + 55)/10)) \\ b_n (V) &= .125 \exp(-(V + 65)/80) \end{split}$$

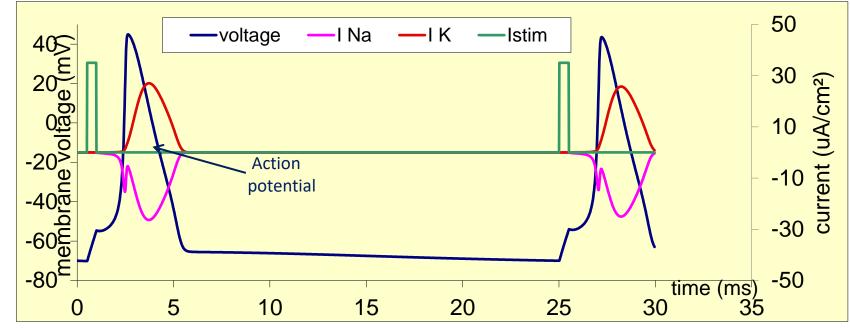


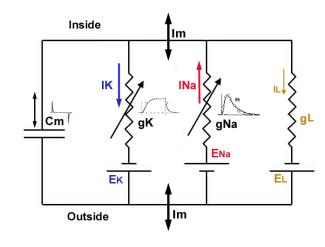


Peripheral Nerve Stimulation and modelling

Physical constraints – Example: Hodgkin Huxley

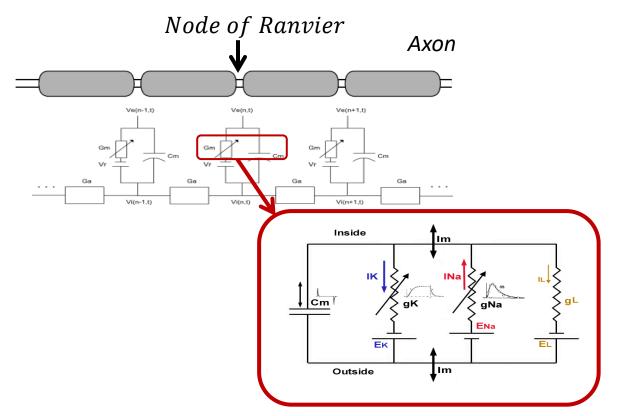
$$\begin{split} C \frac{dv}{dt} &= I - g_{Na} m^3 h (V - V_{Na}) - g_K n^4 (V - V_K) - g_L (V - V_L) \\ \frac{dm}{dt} &= a_m (V) (1 - m) - b_m (V) m \\ \frac{dh}{dt} &= a_h (V) (1 - h) - b_h (V) h \\ \frac{dn}{dt} &= a_n (V) (1 - n) - b_n (V) n \\ a_m (V) &= .1 (V + 40) / (1 - \exp(-(V + 40) / 10)) \\ b_m (V) &= 4 \exp(-(V + 65) / 18) \\ a_h (V) &= .07 \exp(-(V + 65) / 20) \\ b_h (V) &= 1 / (1 + \exp(-(V + 35) / 10)) \\ a_n (V) &= .01 (V + 55) / (1 - \exp(-(V + 55) / 10)) \\ b_n (V) &= .125 \exp(-(V + 65) / 80) \end{split}$$



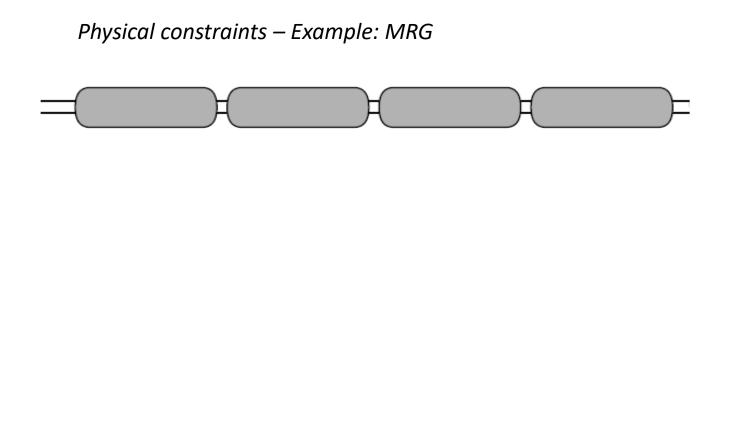


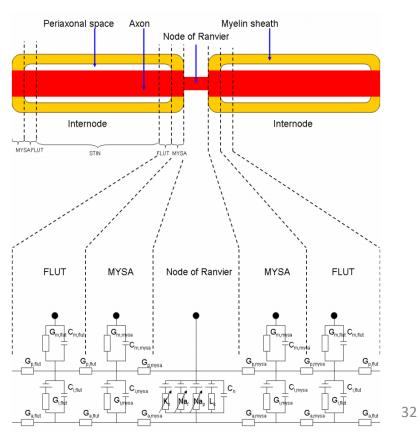
Peripheral Nerve Stimulation and modelling

Physical constraints – Example: Hodgkin Huxley

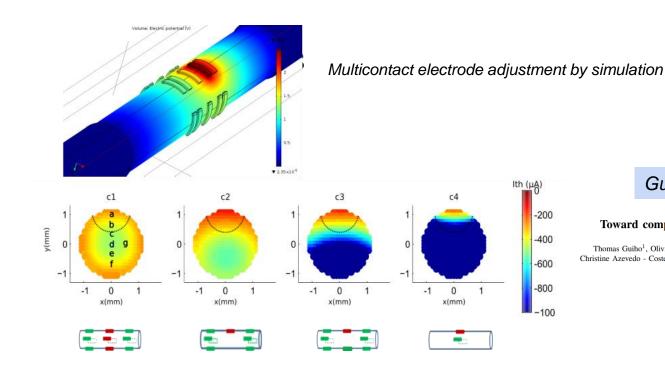


Peripheral Nerve Stimulation and modelling

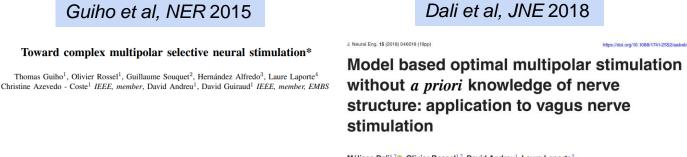




-> A technological solution to the problems of selectivity and invasiveness



- 3D spatial distribution of stimulation currents
- Model-based presets for clinical application



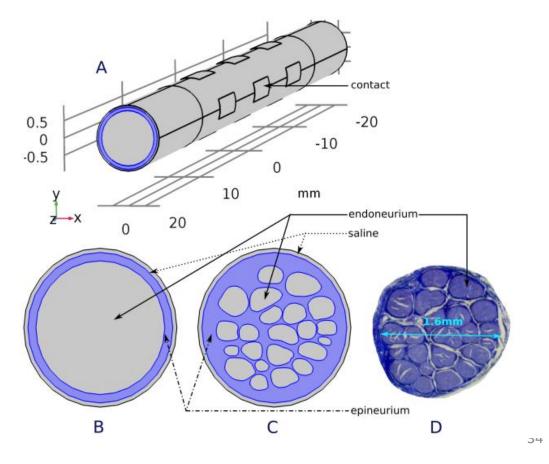
Mélissa Dali^{1,7}, Navid Andreu¹, Laure Laporte², Alfredo Hernández³, Jérémy Laforet^{1,4}, Eloi Marijon⁵, Albert Hagège⁵, Maureen Clerc⁶, Christine Henry² and David Guiraud¹

-> A technological solution to the problems of selectivity and invasiveness

Parametric Identification and validation

Example: Fascicles – interindividual variability and No prior knowledge –

Impact of fasciculariaation - cross-section sudy (x and y)

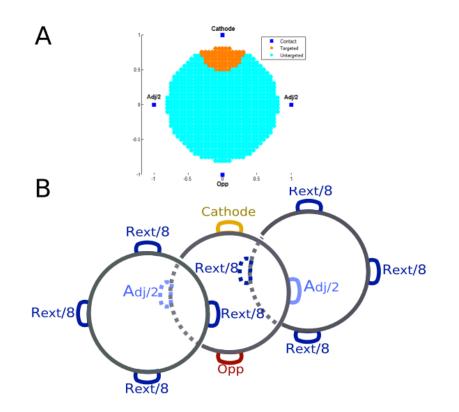


-> A technological solution to the problems of selectivity and invasiveness

Parametric Identification and validation

Example:

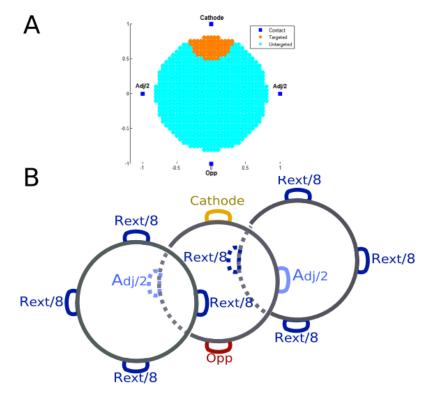
Electrode design distribution of contacts along the x, y and z axes



-> A technological solution to the problems of selectivity and invasiveness

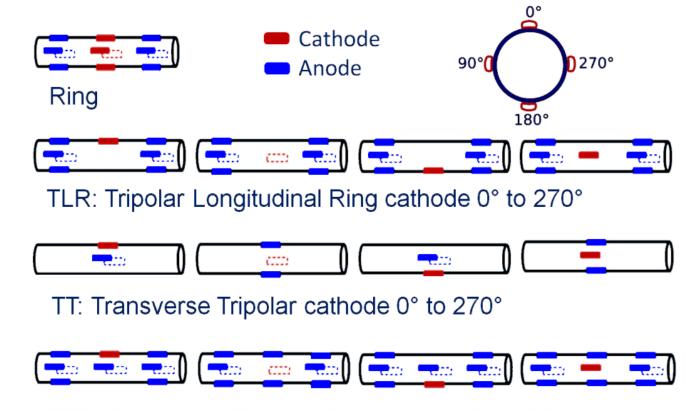
Interest of the Model:

-> Testing a large number of configurations in silico -> Reduce the field of possiblities -> Compliance with the 3R for the use of animals in research



Multi-contact cuff electrode

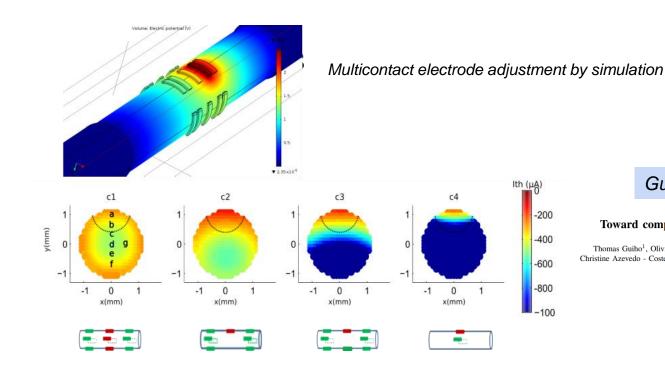
-> A technological solution to the problems of selectivity and invasiveness



TTR: Transverse Tripolar Ring cathode 0° to 270°

Multi-contact cuff electrode

-> A technological solution to the problems of selectivity and invasiveness



- 3D spatial distribution of stimulation currents
- Model-based presets for clinical application

Menssa Danno, Onvier Hossen, David Andreu , Laure Laporter, Alfredo Hernández³, Járémy Laforet^{1,4}, Eloi Marijon⁵, Albert Hagège⁵, Maureen Clerc⁶, Christine Henry² and David Guiraud¹

Assessment of the approach

-> Selective configuration -> Animal experiments

Dali et al, PlosOne 2019

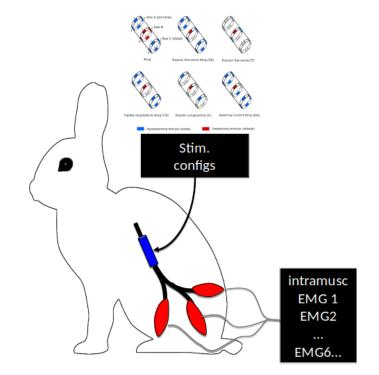
PLOS ONE

PUBLISH ABOUT

Relevance of selective neural stimulation with a multicontact cuff electrode using multicriteria analysis

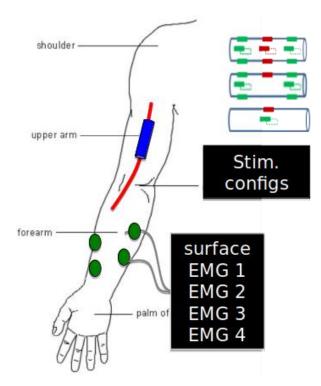
Mélissa Dali, Lucie William, Wafa Tigra, Hubert Taillades, Olivier Rossel, Christine Azevedo 🖬, David Guiraud

Published: July 2, 2019 • https://doi.org/10.1371/journal.pone.0219079



Assessment of the approach

-> Selective configuration -> Animal experiments



Tigra et al, JNER 2020

ClinicalTrials NCT03721861

BMC Part of Springer Nature

Journal of NeuroEngineering and Rehabilitation

Research | Open Access | Published: 19 May 2020

Selective neural electrical stimulation restores hand and forearm movements in individuals with complete tetraplegia

Wafa Tigra, Mélissa Dali, Lucie William, Charles Fattal, Anthony Gélis, Jean-Louis Divoux, Bertrand Coulet, Jacques Teissier, David Guiraud 🖂 & Christine Azevedo Coste

Journal of NeuroEngineering and Rehabilitation 17, Article number: 66 (2020) Cite this article

Agilis project: Offering an implanted solution for upper limb restoration using electrical stimulation



Constraints :

- As less invasive as possible (surgical procedure)
- As efficient as possible (precision of gestures)
- Lessons from FreeHand

Context:

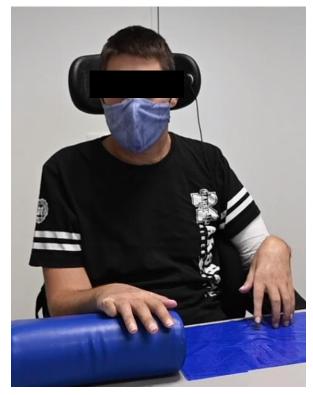
Tétraplegia: Complete lesion of the spinal cord at cervical level, resulting in paralysis of all four limbs.

Aim: Restore wrist and finger movement

- Grip objects independently
- Improved quality of life

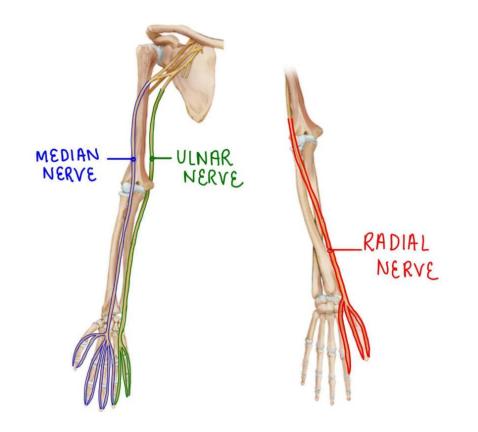
Collaboration with start-up Neurinnov

-> Development and marketing of an active implantable medical device: Neuroprosthesis



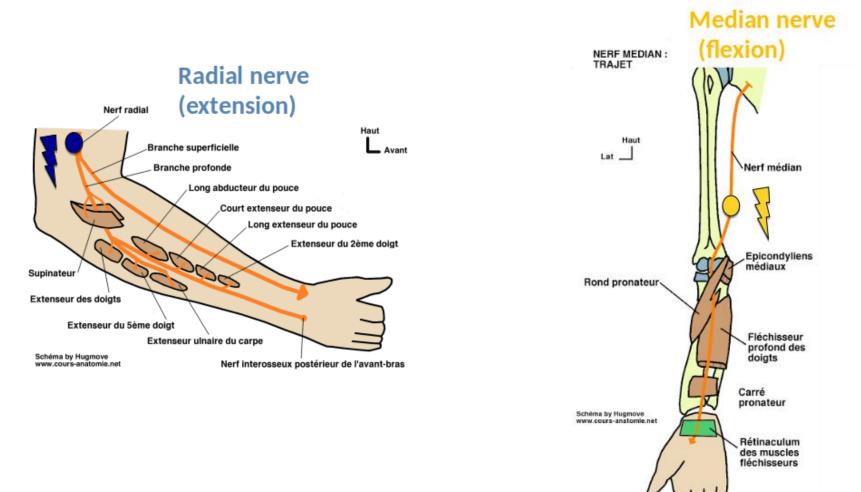
C4 AIS A spinal-cord injured patient

Neurophysiology of the upper limb - In (very) brief

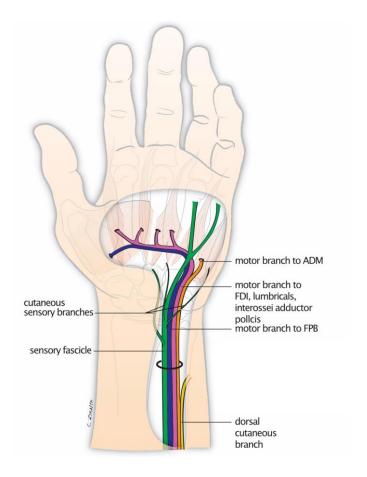


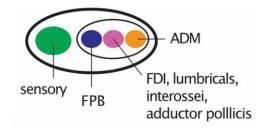
Sensation		Motor Function	
Radial Nerve		Radial Nerve	
Median Nerve Palpate webbing space between thumb and index finger, including palmer surface of hand	ANA H	<u>Median Nerve</u> The ability to bring thumb and little finger together so they are touching	
<u>Ulna Nerve</u> Palpate between little finger and distal ring finger on palmar and dorsal surface of hand		<u>UIna Nerve</u> The ability to abduct all fingers	

Neurophysiology of the upper limb - In (very) brief



Neurophysiology of the upper limb - In (very) brief





Caracteristic:

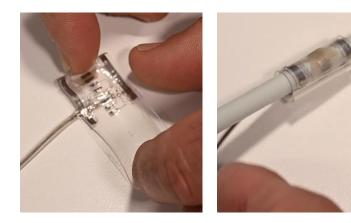
 Topological and functional organisation of nerve fibres

Consequence:

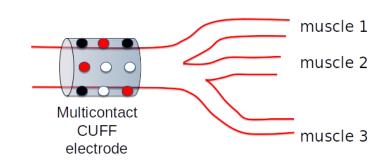
- Possibility of reducing the number of electrodes...
- While retaining motor selectivity

Multicontact cuff electrode

-> A technological solution to the problems of selectivity and invasiveness





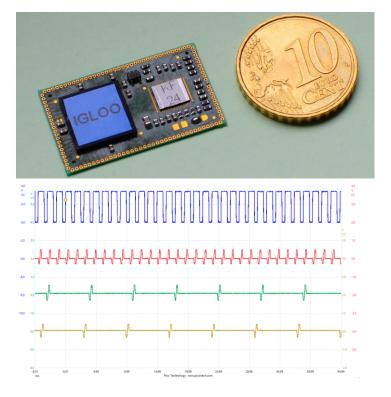


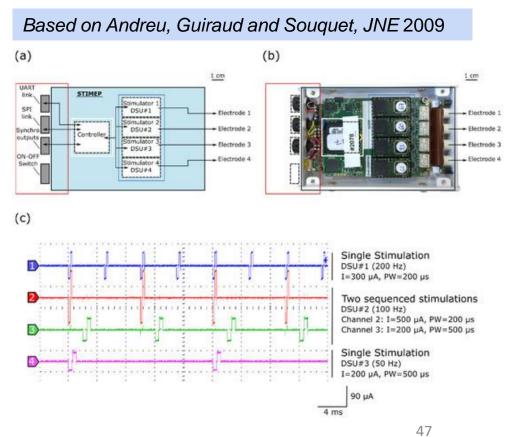


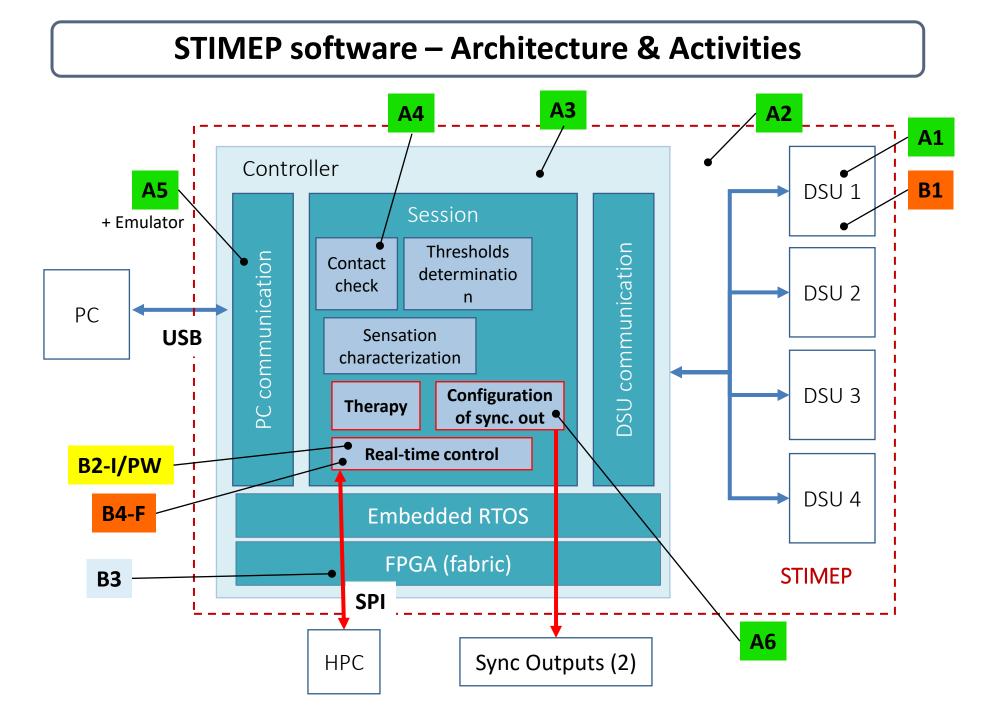
Selective stimulation approach

-> Multicontact cuff electrode and stimulation device

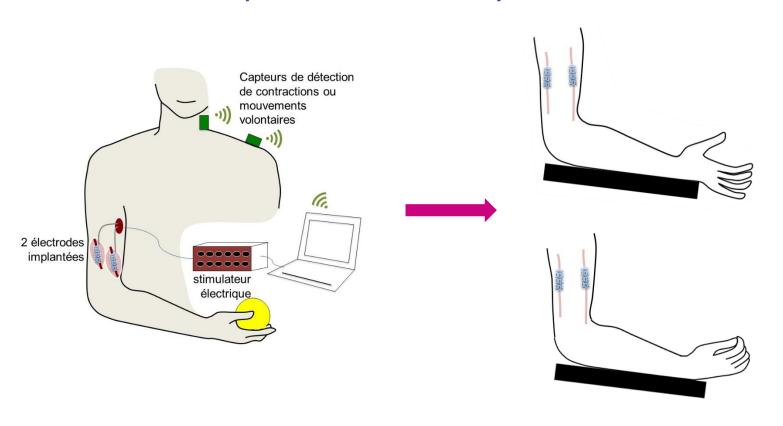




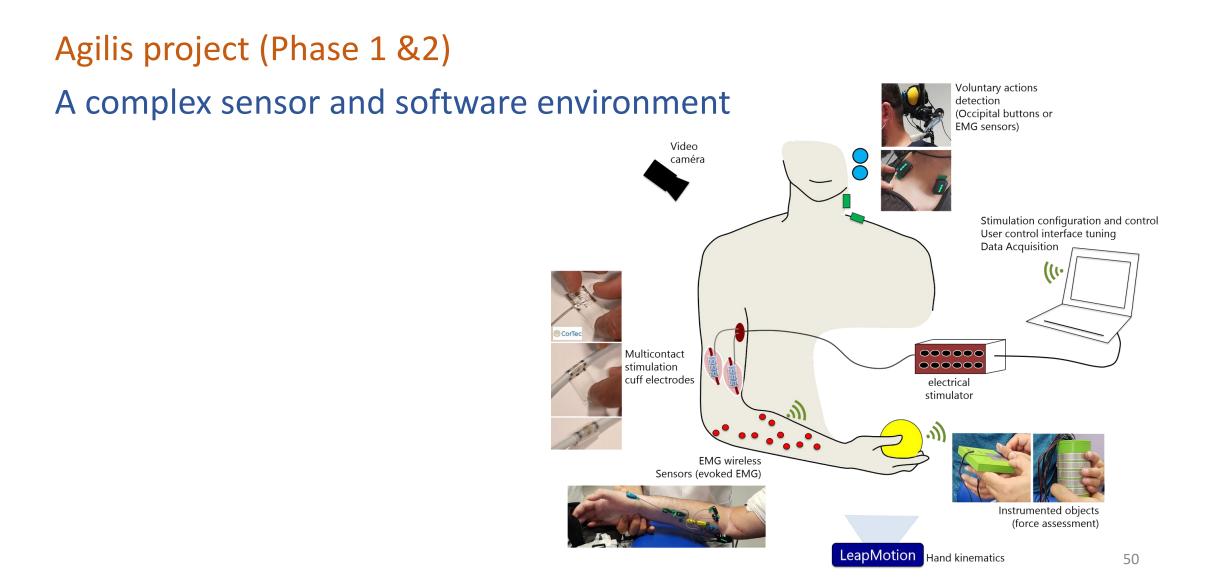


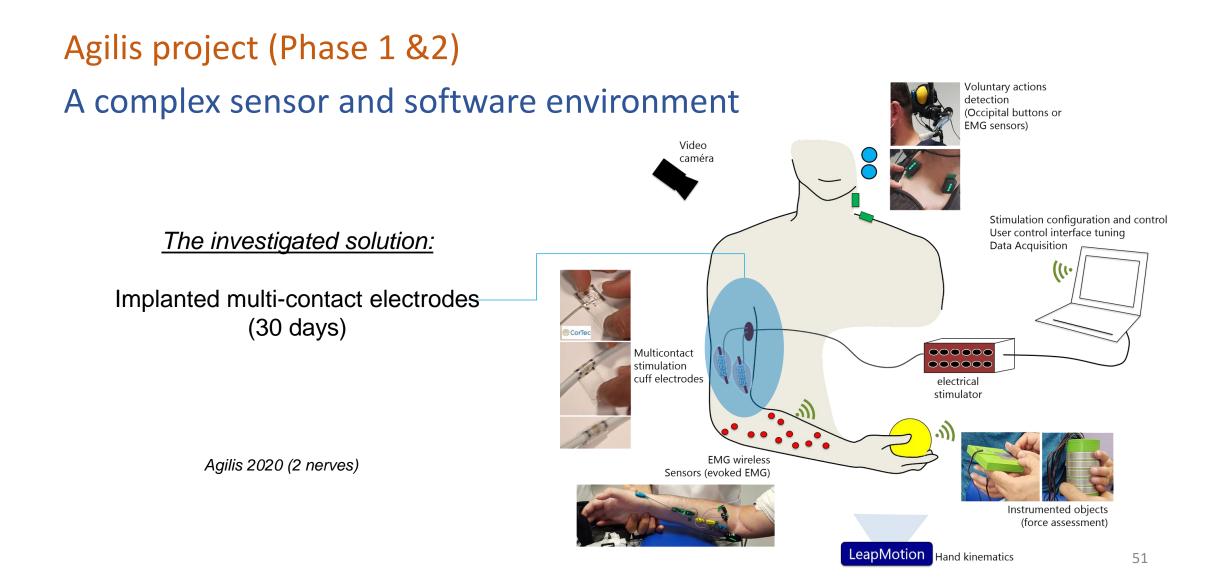


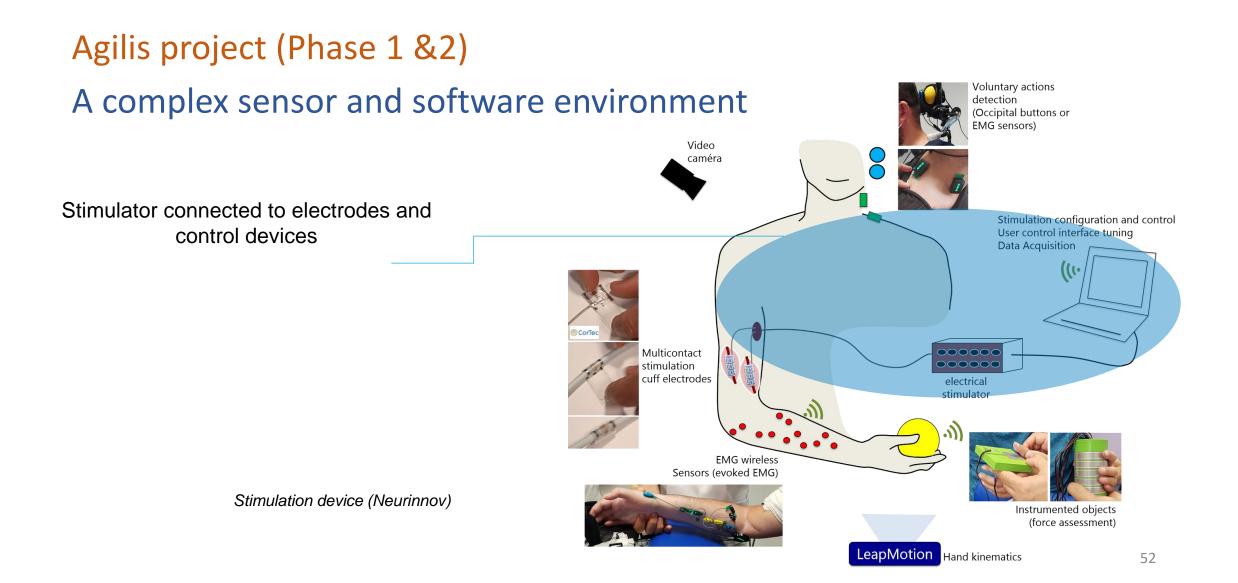
Agilis project (Phase 1 & 2) Schematic operation of the system

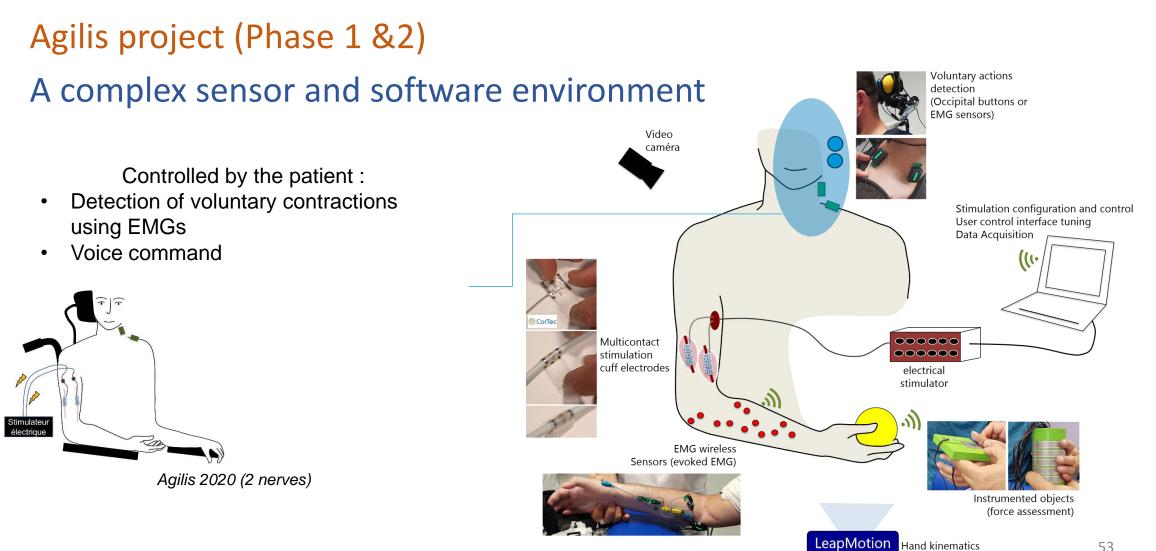


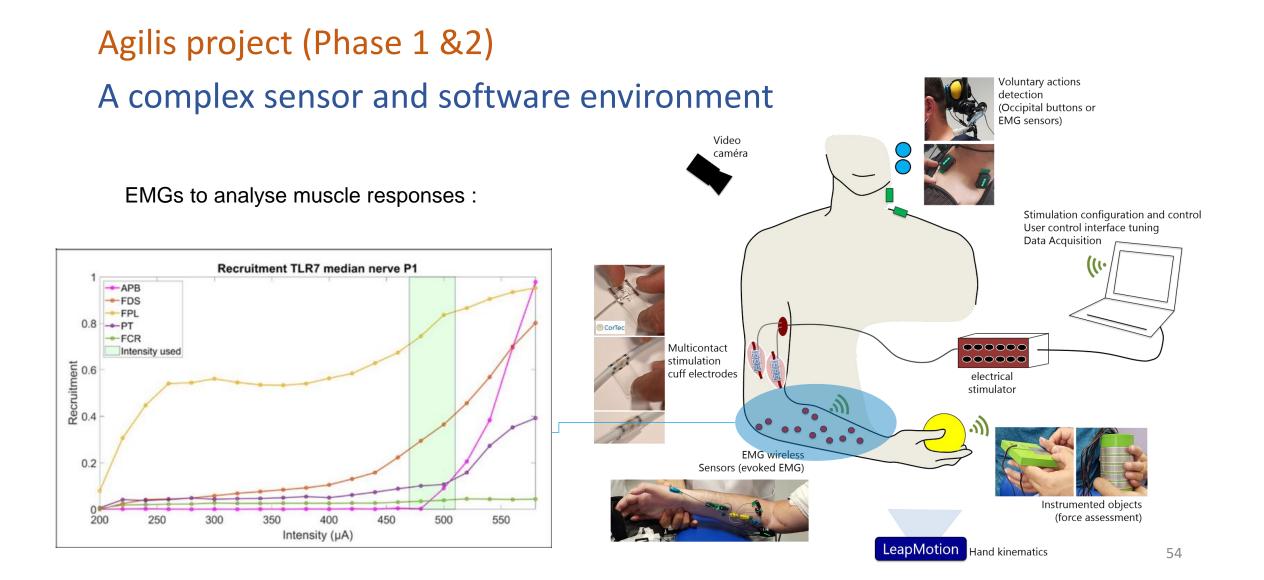
- The patient controls the stimulator using residual movements
- Restoration of hand opening and grasping of objects
- 4 Patients

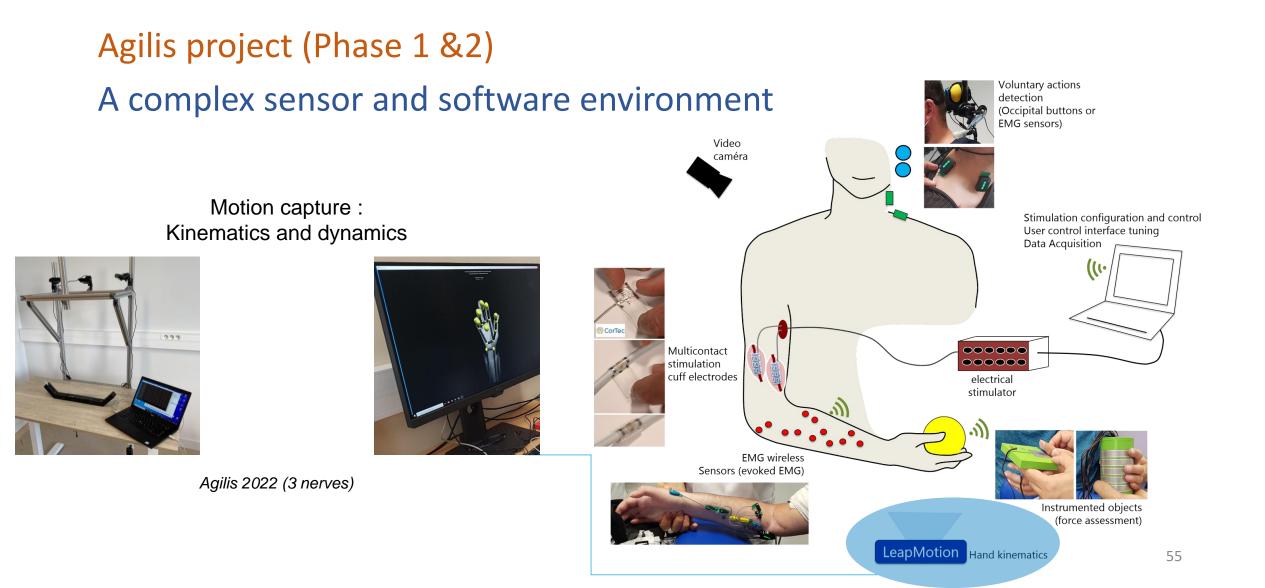


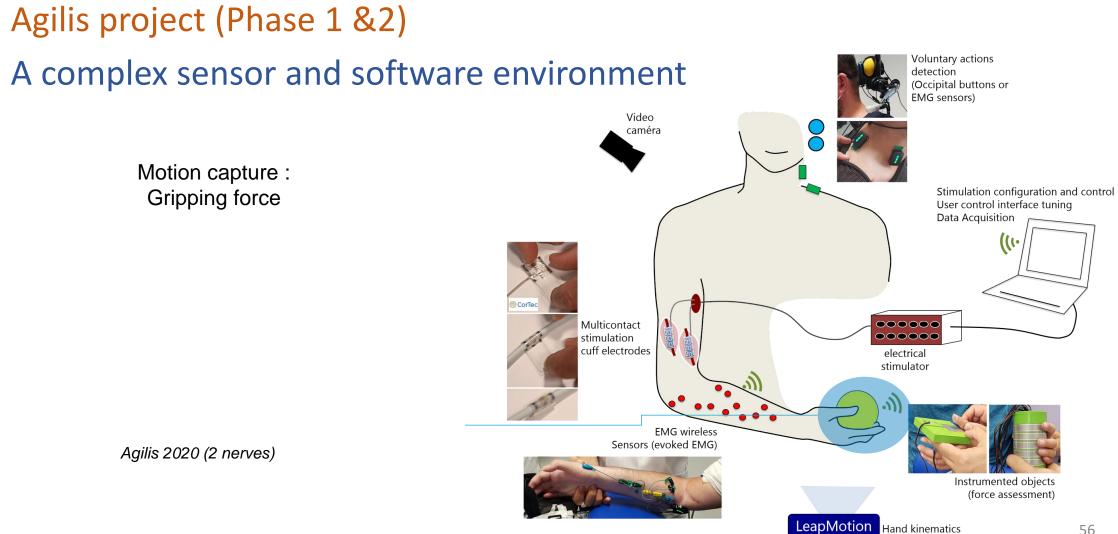












Agilis project – Phase 2 *Results (2020)*

Introduction Domains Marketed Perspectives Beyond

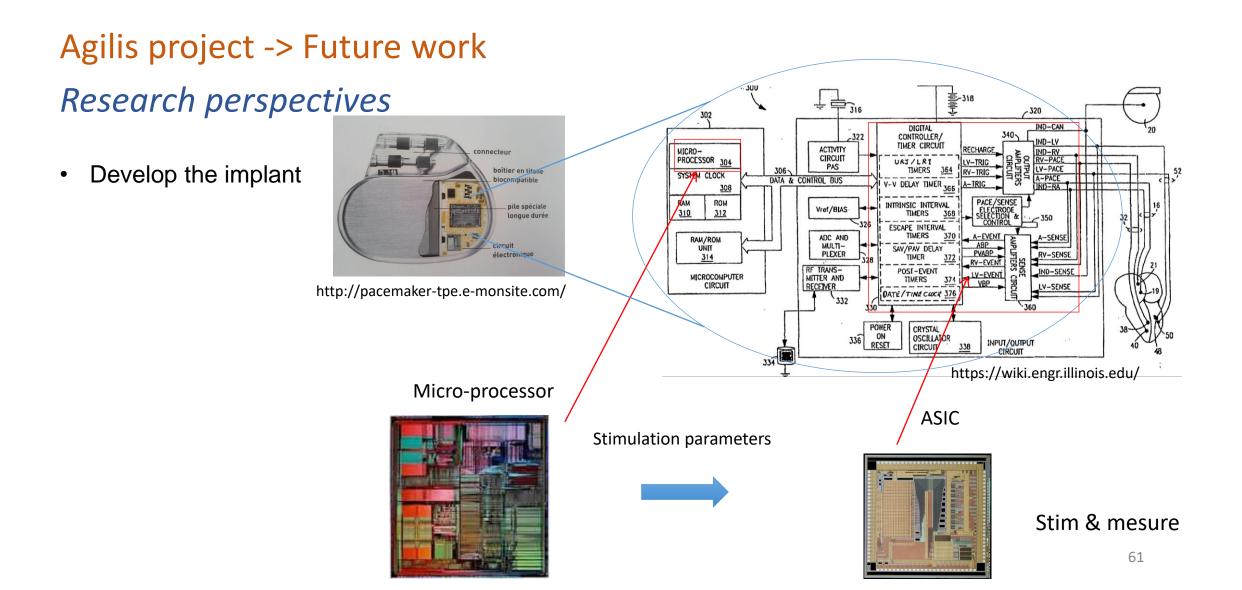
Agilis project – Phase 2 *Results (2023)*

Introduction Domains Marketed Perspectives Beyond

Agilis project – Phase 2 *Results (2023)*

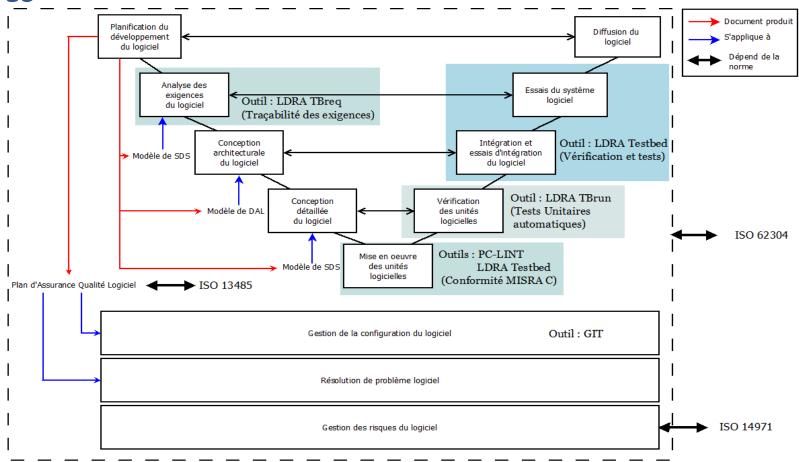
Agilis project -> Future work Research perspectives

- Looking for even greater selectivity (3rd nerve, advanced stimulation strategies)
- Automate stimulation according to the objects approached by the patient's hand (camera in hand)
- Automatic selection of stimulating configurations thanks to on-line biomechanical analysis of movements
- Optimum on-line control, computer vision, etc.



Agilis project -> Future work

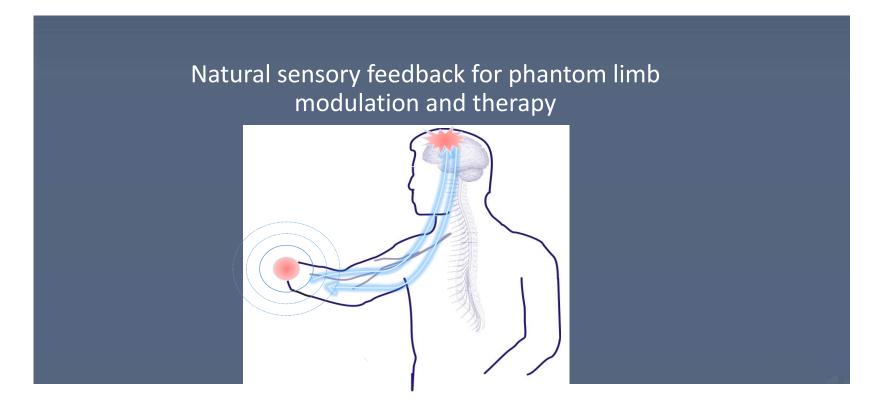
Research perspectives



Peripheral Nerve Stimulation

Intrafascicular electrodes

Intrafascicular Electrodes - Phantom limb pain management



Intrafascicular Electrodes - Phantom limb pain management

EPIONE: Sensory feedback for phantom limb modulation and therapy

Observation:

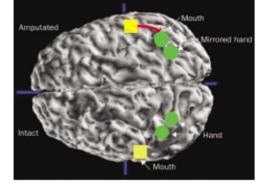
- Amputation \rightarrow Reduction or loss of sensory feedback

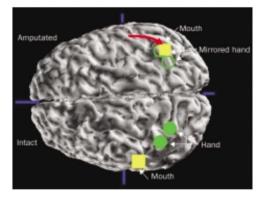
 \rightarrow Changes in cortical representation

 \rightarrow Development of neuropathic pain

Hypothesis:

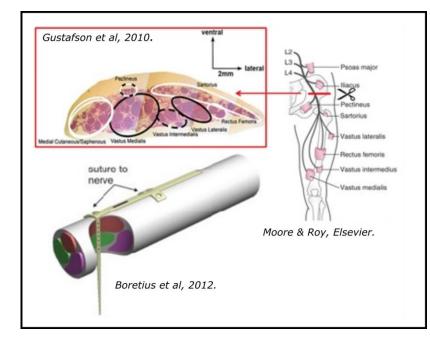
- Research project → Stimulation to replace the sensory feedback
 - \rightarrow Revert the cortical representation
 - \rightarrow Back to a normal representation
 - ightarrow Phantom limb pain reduction

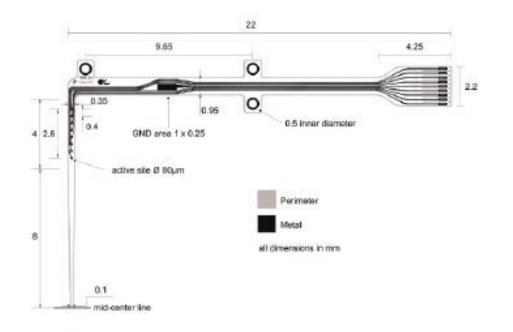




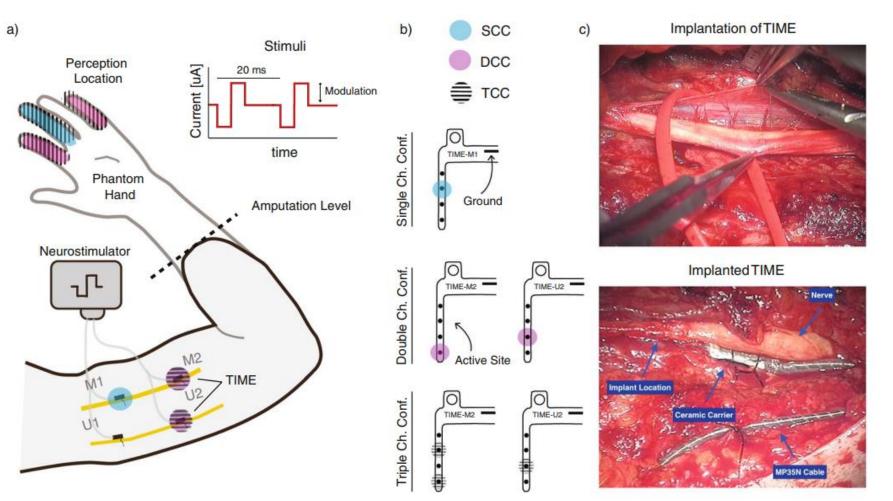
TIME electrode

-> An other technological solution to the problems of selectivity and invasiveness

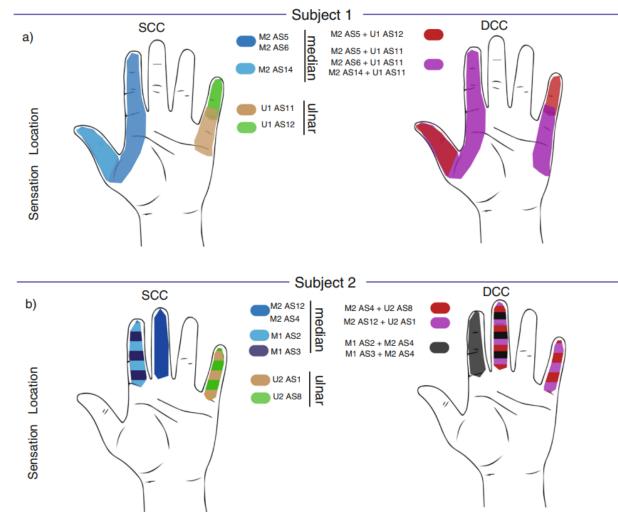




Phantom limb pain management



Phantom limb pain management



Spinal cord Stimulation

In a context of SCI

Spinal cord

<u>Protected by the spine (vf – la colonne vertebrale)</u>

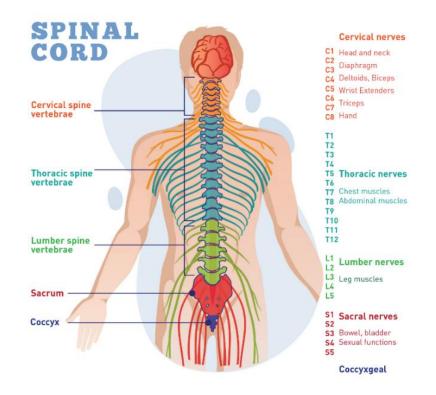
- Pre-existing neural networks
- First level of signal processing (reflexes etc.)

Its functional unit

- The spinal level (*vf le niveau medullaire*)
 - -> Dedicated to a specific territory (C4 level for example)
 - -> Spreads the motor command
 - -> Gathers sensitive information from the periphery

In case of spinal cord injury

- Communication breakdown between the brain and the periphery
- Motor and sensitive impairments below the lesion
- Sublesional spinal networks: Intact but loss of supraspinal driving command
 - -> Spinal cord stimulation for reactivation?



Spinal cord – The spinal level

Anatomically

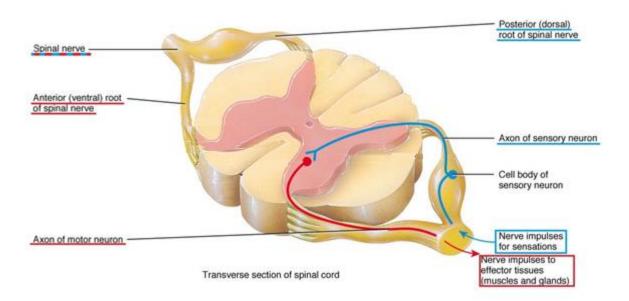
- Grey matter
 - -> Cell body packed within the cord in a butterfly shape
- White matter
 - -> Nervous fibres at the periphery gathered in tracts

Functionally

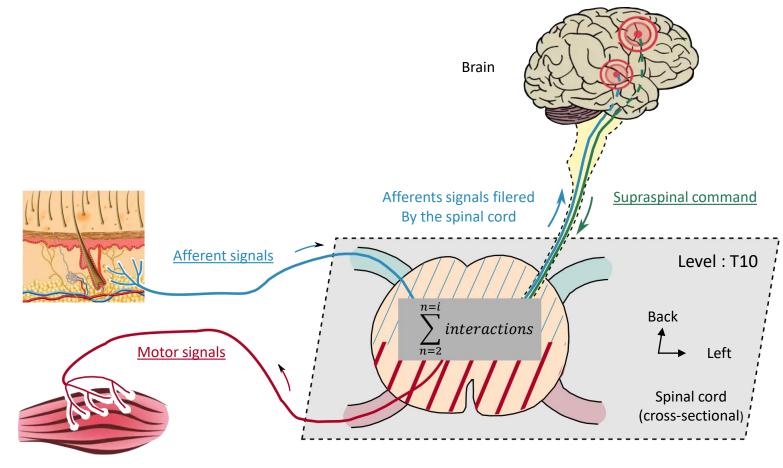
- Dorsal spinal cord and dorsal root -> exclusively sensitive
- Ventral spinal cord and ventral root -> exclusively motor
- Left side -> left part of the body / Right side -> right part

Spinal cord stimulation

- Promote spinal cord excitability by dorsal stimulation
 - -> Spectacular results in the past few years in person with SCI
 - -> Partial functional and volitional recovery



Spinal cord – Multiple interactions



Dorsal = sensory

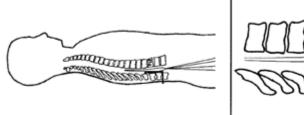


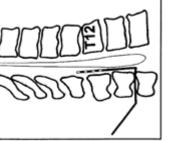
Ventral = motor

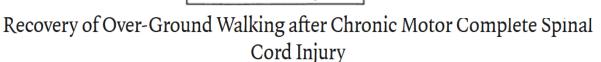
n=i 'interactions, with n: number of neurons n=2

Improvements of motor tasks after spinal cord injuries: SCS + Training

-> Epidural stimulation + Intense locomotor treadmill training







Claudia A. Angeli, Ph.D., Maxwell Boakye, M.D., Rebekah A. Morton, B.S., Justin Vogt, B.S., Kristin Benton, B.S., Yangshen Chen, Ph.D., Christie K. Ferreira, B.S., and Susan J. N Engl | Med 2018; 379:1244-1250 September 27, 2018 Harkema, Ph.D.

-> Transcutaneous stimulation + Training for grip strength

Gad P, Lee S, Terrafranca N, Zhong H, Turner A, Gerasimenko Y and Edgerton V R 2018 Non-invasive activation of cervical spinal networks after severe paralysis *J. Neurotrauma* 35 2145–58

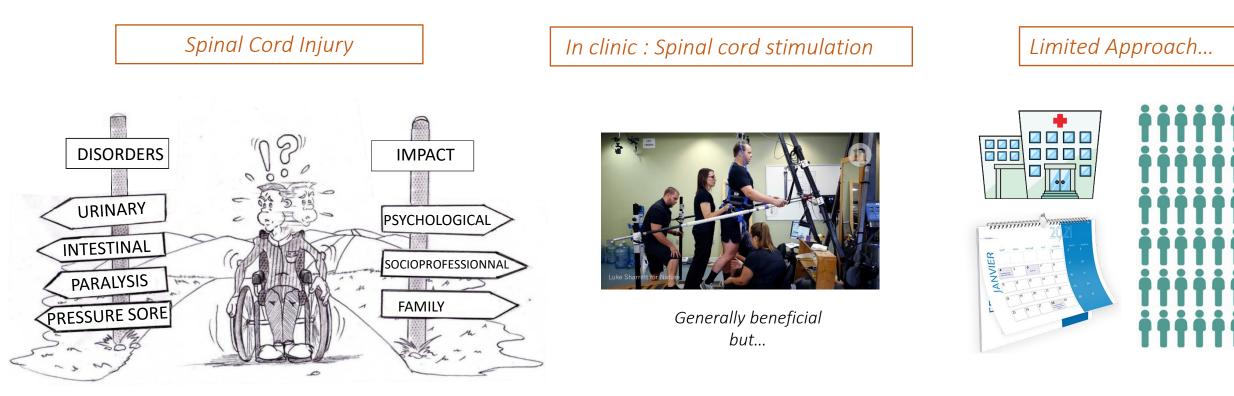
Training:

--> Provide task-specific afferent feedback

Stimulation:

- --> Potentiate spinal cord excitability
 - Mechanism of action of SCS -> potentiate afferences
 - Interaction SCS <-> supraspinal input -> Boost plasticity

Spinal cord stimulation



Limited... in its current form because empirical...

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Spinal cord stimulation - illustration of the approach

Article

The neurons that restore walking after paralysis

1) The journal

nature

Aims & Scope

Nature is a weekly international journal publishing the finest peer-reviewed research in all fields of science and technology on the basis of its originality, importance, interdisciplinary interest, timeliness, accessibility, elegance and surprising conclusions. Nature also provides rapid, authoritative, insightful and arresting news and interpretation of topical and coming trends affecting science, scientists and the wider public.

2021 Journal Metrics

2 year Impact Factor (2021) - 69.504

5- year Impact Factor (2021) - 63.580

Immediacy index - 17.085

Eigenfactor® score - 1.11428

Article Influence Score - 25.568

2-year Median - 31

2) The authors

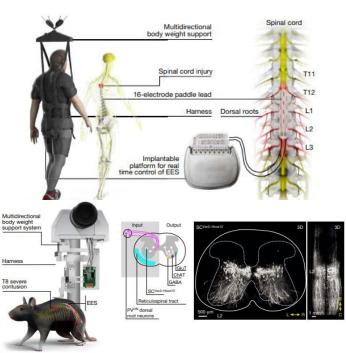
Claudia Kathe^{1,2,3,9}, Michael A. Skinnider^{1,4,9}, Thomas H. Hutson^{1,2,3,9}, Nicola Regazzi^{1,2,3}, Matthieu Gautier^{1,2,3}, Robin Demesmaeke^{1,2,3}, Salif Komi^{1,2,3}, Steven Ceto^{1,2,3}, Nicholas D. James^{1,2,3}, Newton Cho^{1,2,3}, Laetitia Baud^{1,2,3}, Katia Galan^{1,2,3}, Kaya J. E. Matson⁵, Andreas Rowald^{1,2,3}, Kyungjin Kim⁶, Ruijia Wang^{1,2,3,7}, Karen Minassian⁸, John O. Prior⁷, Leonie Asboth^{1,2,3}, Quentin Barraud^{1,2,3}, Stéphanie P. Lacour⁶, Ariel J. Levine⁵, Fabien Wagner^{1,2,3}, Jocelyne Bloch^{1,2,3,10^{III}}, Jordan W. Squair^{1,2,3,10^{III}} & Grégoire Courtine^{1,2,3,10^{III}}

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IR Minev, P Musienko, A	Electronic dura mater for long-term multimodal neural interfaces R Minev, P Musienko, A Hirsch, Q Barraud, N Wenger, EM Moraud, Science 347 (6218), 159-163			2015	
	ring voluntary control of locomotion after paralyzing spinal cord injury 821 2012 den Brand, J Heutschi, Q Barraud, J DiGiovanna, K Bartholdi, 336 (6085), 1182-1185				
input	onfunctional spinal circuits into functional states after the loss of b inko, R Van Den Brand, A Yew, P Musienko, (10), 1333-1342	orain	754	2009	

3) The paper

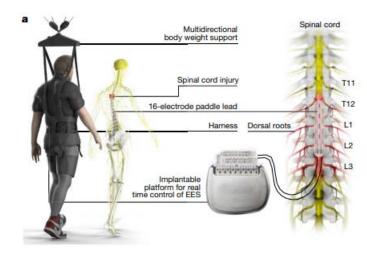
Nature | Vol 611 | 17 November 2022 No keyword section



Spinal cord stimulation - illustration of the approach

<u>9 Participants: 2 Groups</u> *Clinical study (STIMO): EES Rehab protocol = Closed-loop EES + neurorehab w/ support (4 or 5/week)*

Participants	Implant	Acute phase	After 5 months of EES Rehab
Group A: N=6; Severe or complete motor paralysis but some degree of sensation in the legs	Full Medtronic (Pain relief) + (DBS) + WB (Custom Wireless Bridge)	1) « EES immediatly enabled to improve or regain ability to walk while supported in the robotic interface »	 Weight-bearing capacities improved considerably over time, which enabled the participants to walk outdoors with <i>EES^{ON}</i> and an assistive device for stability » Participants who
Group B: N=3; Complete sensorimotor paralysis	Uter State of the	2) « Volitional control over the amplitude of their steps w/ EES » (except 1 from Group B)	exhibited residual functions before EES displayed an increase in motor scores » + « walking in absence of EES in 4 participants»





Spinal cord stimulation - illustration of the approach

<u>9 Participants: 2 Groups</u> *Clinical study (STIMO): EES Rehab protocol = Closed-loop EES + neurorehab w/ support (4 or 5/week)*

Immediate effect – Acute phase

Biomimetic EES protocols immediately enabled all nine participants to improve or regain the ability to walk while supported in the robotic interface (Extended Data Fig. 1a). Moreover, the participants, including two with complete sensorimotor paralysis, could exert volitional control over the amplitude of their steps when EES was turned on (Extended Data Fig. 1b).

EES^{REHAB} restores walking in 9 humans with chronic spinal cord injury



Thank you for your attention